

# Robotic Training System for Upper Limb Rehabilitation<sup>1</sup>

## Plataforma Robótica para la rehabilitación de miembros superiores<sup>2</sup>

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## Abstract

*Background:* Robot-assisted therapy or exoskeleton is an active mechanical device that can be easily adjusted to fit a different patient limb length, and is able to coordinate and amplify movements. The aim of this study focuses on developing a robotic training system and quantification methods for upper limbs rehabilitation in clinic environments to be used in survivor stroke patients with motor disorders or loss of physical strength on one side of the body. *Methods:* From an integrated approach, a design of one exoskeleton is presented which allows patients perform complex movements in four degrees of freedom (DOF) rehabilitation system. The system is controlled by means of user interface developed with Lab view v8.6 software that supports control and user interaction with the exoskeleton; so it's possible for therapist to modify the patient routine including new movements and a number of repetitions in articulating joints of shoulder, elbow and wrist. On other hand system permits bio-feedback of electromyogram patient activity during rehabilitation sessions. *Results:* Biomechanical analyses and structure design, implementation of power systems, the development of the control system and user interface as well as its integration with the mechanical system is presented. *Conclusions:* A robot arm exoskeleton device with four DOF; able to develop complex, accurate and repetitive therapeutic routines for articulating joints of shoulder, elbow and wrist through an interface is shown. The device permits to follow chronologically patient outcomes recording the electromyogram activity during rehabilitation progress.

## Keywords

biomechanics; exoskeleton; electromyographic signal

## Resumen

*Introducción:* Un exoesqueleto se conceptualiza como un mecanismo estructural externo cuyos segmentos y articulaciones se corresponden con las del cuerpo humano y es capaz de coordinar y amplificar sus movimientos. El objetivo del trabajo se enfoca en desarrollar una tecnología de plataforma robótica de asistencia y métodos de cuantificación para la rehabilitación motora de miembros superiores en ambientes clínicos y ambulatorios para pacientes con afecciones motoras como resultados de enfermedades cerebrovasculares. *Métodos:* Se presenta a partir de una concepción integradora el diseño del prototipo de un exoesqueleto que permite al paciente realizar movimientos combinados a partir de los cuatro grados de libertad que provee el dispositivo de rehabilitación. El sistema es controlado por medio de una interfaz de usuario desarrollada en Labview que soporta el control e interacción del usuario con el exoesqueleto, lo cual posibilita que el terapeuta puede modificar la rutina que debe realizar el paciente incluyendo nuevas trayectorias y el número de repeticiones a seguir por el exoesqueleto en las articulaciones de hombro, codo y muñeca. Adicionalmente, posibilita la retroalimentación visual de la actividad electromiográfica del paciente durante la rehabilitación. *Resultados:* Se presenta el diseño mecánico de la armadura, implementación de los sistemas de potencia, el desarrollo del sistema de control y de la interfaz de usuario así como su integración con el sistema mecánico. *Conclusiones:* Se desarrolla y pone en funcionamiento una avanzada plataforma robótica capaz de desarrollar diversas rutinas terapéuticas combinando 4 grados de libertad en hombro, codo y muñeca, capaz de controlar a través de la interfaz desarrollada desplazamientos regulados, exactos y repetitivos, así como seguir cronológicamente la evolución del paciente registrando la actividad mioeléctrica durante el proceso de rehabilitación.

## Palabras clave

Biomecánica; exoesqueleto; señal electromiográfica; control activo y pasivo

## Introduction

There are several diseases and physical trauma, such as brain injury and leaving motor deficits in the upper extremities of individuals; these injuries which require specialized rehabilitation treatment with physiotherapy sessions conducted by expert personnel. Stroke is one of the most important problems in the developed world and in Cuba, where occupies the third leading cause of death (8891 deaths in 2012) and second only to cardiovascular disease and cancer (Estevez, 2012). From 50-70% of cases suffers sequels, about a third of stroke survivors are unable to fend for themselves and approximately 75% lose their skills to return to work.

Today, most of these therapies are performed by the physiotherapist manually and involve movements in routines that require physical effort from the specialist, which may cause the end of a day the physiotherapist, the effects physical fatigue, not properly performing the qualitative and quantitative methods; all of which affects the durability, efficiency and even full recovery.

Exoskeletons mechanical development is the topic of many medical investigations. Its applications include a wide spectrum ranging from the rehabilitation process of patients to replacement of vital functions, such as walking in people with permanent conditions (Hui, 2009; Staubli, 2009; Lo, 2011).

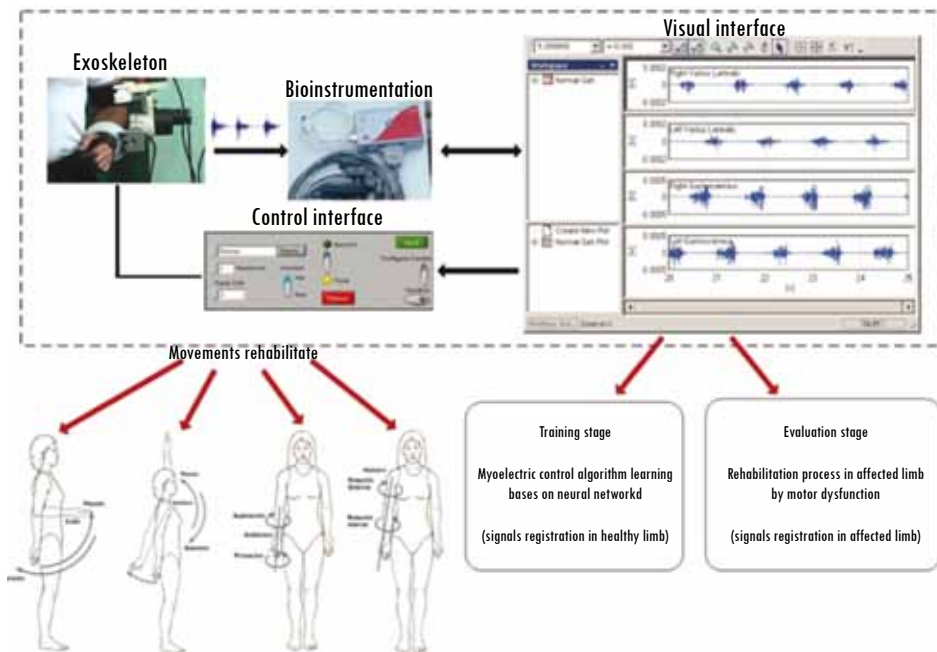
The paper presents the development of a robotic platform that enables the realization of passive movement therapy and active rehabilitation in the upper limb in a controlled and repeatable way that could keep a log of patient outcome.

## 1. Methods

The design stages are related to: mechanical design of the prototype or framework, the design of bioinstrumentation system, developing software platforms for the acquisition of bioelectric signals and actuator control devices as well as the development of the system controlling the power for the exoskeleton's operation (Aguirre and Colgate, 2010; Cenciarini and Dollar, 2011; Wege and Zimmermann, 2007).

Figure 1 presents the proposed rehabilitation of upper platform for passive and active modes of upper limb control. A segmented into two blocks visual interface allows the control of exoskeleton based on motion routines for programming and biofeedback of myoelectric signals acquired during the rehabilitation process, respectively. The signal acquisition is performed through a system designed for this purpose bioinstrumentation. Exoskeleton platform designed and built, is initially designed to operate in passive mode, which is activated by the information related to the motion routines that configure the physical therapist, to perform the therapy. Additionally, the system provides the ability to modify or create new routines and individualized movements for each patient.

Figure 1. Upper limb motor rehabilitation system



### 1.1. Biomechanical study of the upper limb

The proposed system cannot be in conflict with the clinical practice for the recovery of the affected limb and in medical terms is known as the therapeutic routine. Considering the impossibility of satisfying all possible exercises, especially those that incorporate hand movements, which greatly complex design; conceived routine includes movements from 4 degrees of freedom: flexion and

shoulder extension, flexion and elbow extension, forearm supination/pronation and rotation of the humerus.

Whereas the anthropometric characteristics of the patients (weight and height) and according to the work of Braune and Winter (Winter, 1979; Braune, 1988), the locations of the centers of gravity, weight of the arm, forearm and hand were obtained from the that the virtual model of the upper limb is constructed. According to the characteristics of an average patient calculations were performed for people of average weight and height  $H = (1.4 - 1.85) \text{ m}$   $W = (50 - 100) \text{ kg}$ .

**Table 1. Anthropometric data of weight and position of the body segments**

Segment	Segment weight/Total body weight	Center of mass/ segment length	
		Proximal/Distal	
Hand	0.006	0.506	0.494
Forearm	0.016	0.430	0.570
Arm	0.028	0.436	0.564

**Figure 2. Upper limb virtual mode**



For different degrees of freedom the necessary torque to move each joint was calculated assuming an average patient generates a normal torque equal to that calculated by performing a static analysis of the forces at arm's length (Figure 3). The results of the mechanical behavior of each of the upper limb joints are shown in Table 2.

Figure 3. Determination the necessary torque and DOF for each articulation

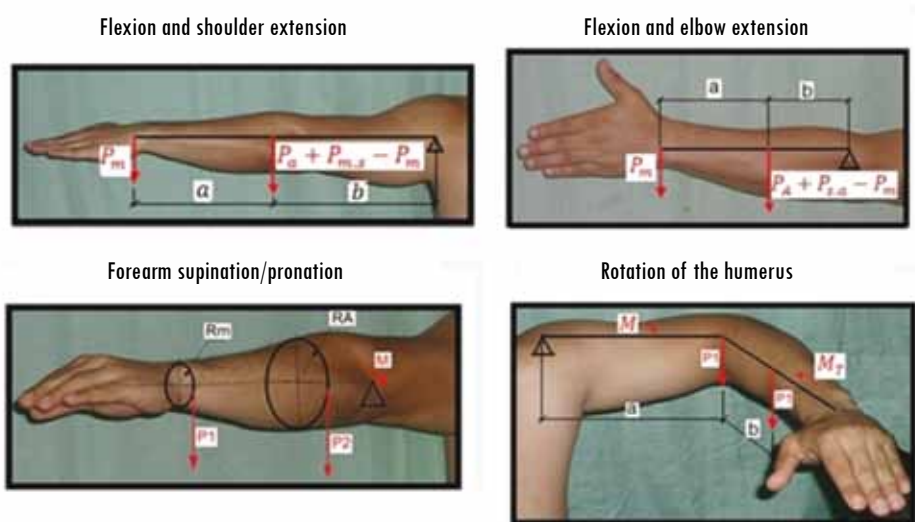


Table 2. Joint torque calculated for each DOF

Total body weight (kg)	Shoulder Flexion/extension torque (Nm)	Elbow Flexion/extension torque (Nm)	Forearm pronation/supination torque (Nm)	Humerus Rotation torque (Nm)
50	13.9	2.75	0.49	9.45
100	27.8	5.50	0.97	18.90

### 1.1.1. Actuator design

Because of the best actuator is the simplest, practical, lightweight and economical, from the results of the biomechanical analysis of the upper extremity, it was decided to consider a design with the use of electric motors, gearboxes and sliding adjustment plates. When considering the torques produced by the weight of the arm and armature the power required moving each joint was determined. In these cases were selected 2-phase stepping motors (Table 3). The maximum speed of each joint was estimated as an average of 25 %/s. from the consensus of the designers and physiotherapists by own peculiarity of the routines used in the rehabilitation of patients.

**Table 3. Requirements for joint power and DOF**

DOF of upper limb	Motor power (W)
Shoulder Flexion/extension	12.00
Elbow Flexion/extension	2.36
Forearm pronation/supination	0.41
Humerus Rotation	9.00

The main geometry and dimensions, material selection and control of the mechanical strength of each of the components of the structure were determined by using the finite element professional package ANSYS MULTIPHASE.

### *1.2. Control system*

The control interface with techniques electromyography biofeedback for the exoskeleton was implemented in Lab VIEW v8.6 software professional. The system integrates a computer bioinstrumentation for electrical activity acquisition in the different upper limb movements. The electronic card and the bioinstrumentation system interact with software in order to control the movements of the exoskeleton routines and display myoelectric activity (biofeedback), respectively.

## **2. Results**

### *2.1. Actuator design*

Considering the requirements and considerations discussed above, as well as the need for the equipment enables the reproduction of the movements and the possible combination of those, present in realistic rehabilitative therapy as well as criteria of strength, low weight, and smooth and quiet operation; it was considered a simple mechanism of gearbox and sliding plates. Actuator was kinematically and structurally capable of responding to the movements involved. Figure 4 shows the correspondence between the proposed design and therapeutic program.

Figures 5 and 6 represent the proposed CAD modeling armature and some of the components as well as meshing by using finite element analysis professional package.

Figure 4. Correspondence between the design and therapeutic routines. (a) Routine that includes shoulder flexion and elbow and wrist pronation-supination. (b) Routine including shoulder extension, elbow flexion and forearm supination-pronation

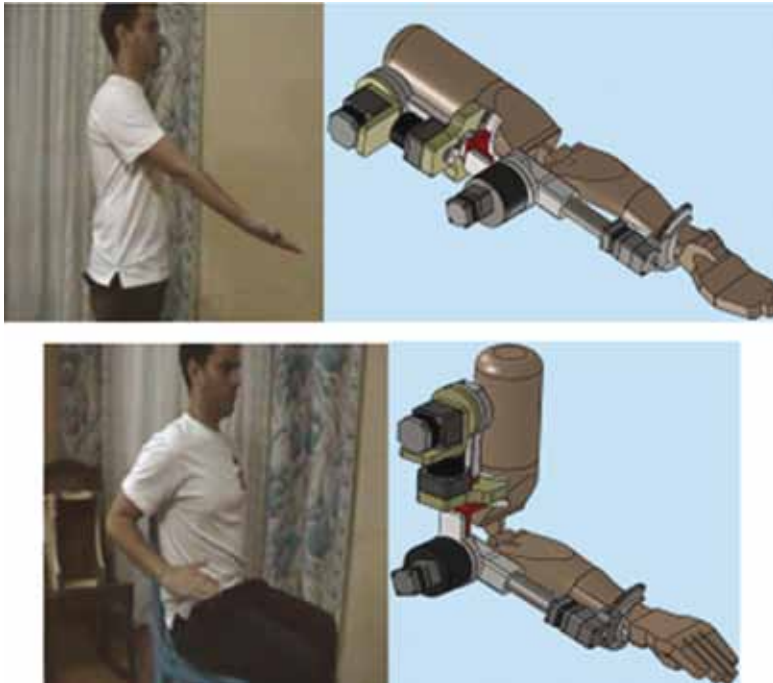


Figure 5. Modeling CAD and meshing exoskeleton armature

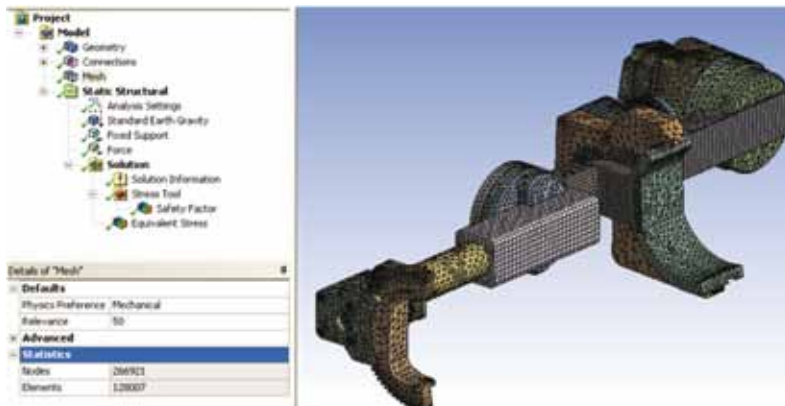
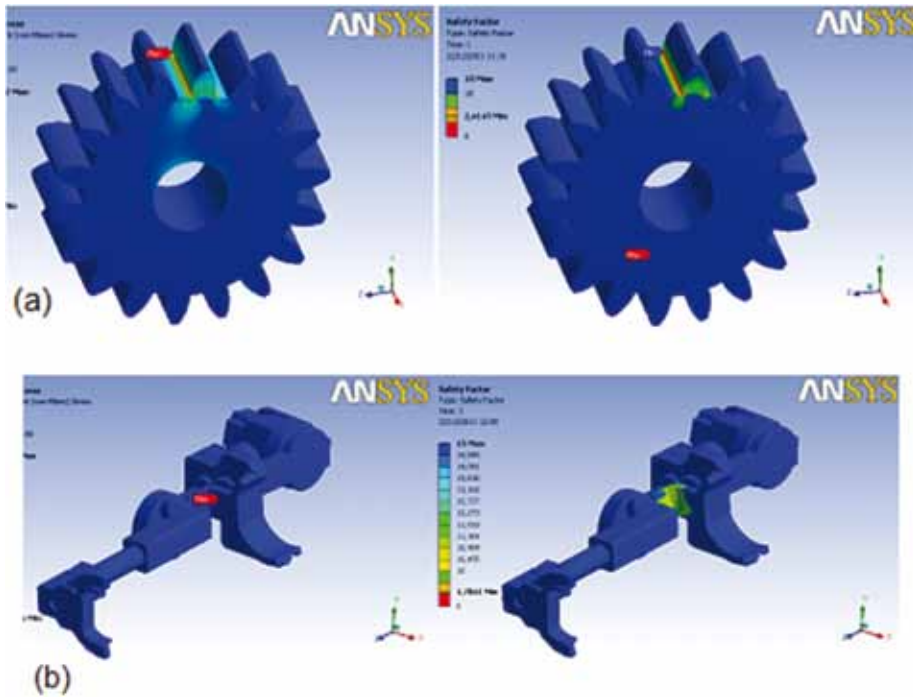




Figure 6. (A) Maximum stresses on the pinion of the humerus rotation mechanism (52.7 MPa). Safety factor of gear, FDS = 2.41. (B) Distribution of stresses ( $\sigma_{\max} = 106.6$  MPa) and safety factor of the framework for the most critical condition in the rehabilitation program (FDS = 1.7)



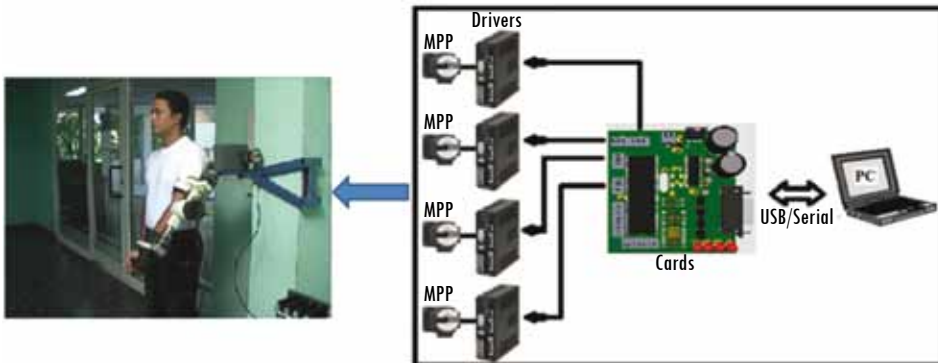
## 2.2. Control system

Biomechanical exoskeleton arm is a part, as seen in Figure 1, of a complex system which is commanded from the patient moving intention information. For this it is necessary to record the muscular electrical signal to the various movements through surface electrodes (Jacob et al., 2001; Safizadeh et al., 2011).

The command and control system are presented in Figure 7. For the electronic driving step motors were chosen (MPP) Bipolar Hybrid-type, due to the operation in micro-step mode, giving the possibility of better control and positioning. Thus offer a better relationship between torque and size/weight.

The controller (driver) was selected the M542 V2.0 type, with high-performance, operating in micro-step technology-based control of a pure sinusoidal current mode. This driver can handle electrical motors with low noise levels and provides better performance at high speeds relative to other commercial drivers. It is suitable for controlling the hybrid step motors 2 and 4 phases, just as the selected.

Figure 7. Exoskeleton control system



The control board with RS232 communication was developed with the purpose of managing via graphical interface the controllers that handle the MPP and was initially simulated virtually by PROTEUS professional package (Figure 8) and was powered by a voltage of 12V direct current. The card incorporates indicators that point to the existence of the supply voltage and the motor in motion. A PIC18LF4620 microcontroller is programmed to make the transfer pulse to the controllers that manage the stepping motors (MPP) of the exoskeleton.

Figure 9 shows the controller and the card M542 developed for the control system.

### 2.2.1. Firmware

The firmware for PIC was implemented using the MPLAB/C18 developing tool; the communication protocol used was as follows:

- Home TX (UN BYTE)
- IP module (DOS BYTES)
- Motor number (UN BYTE)
- Direction (A BYTE)
- Angle (A BYTE)
- FINAL TX (UN BYTE)

Figure 10 shows the flow diagram for configuring and implementing the control in the stepper motors.

Figure 8. Circuit simulated ISIS-PROTEUS card developed

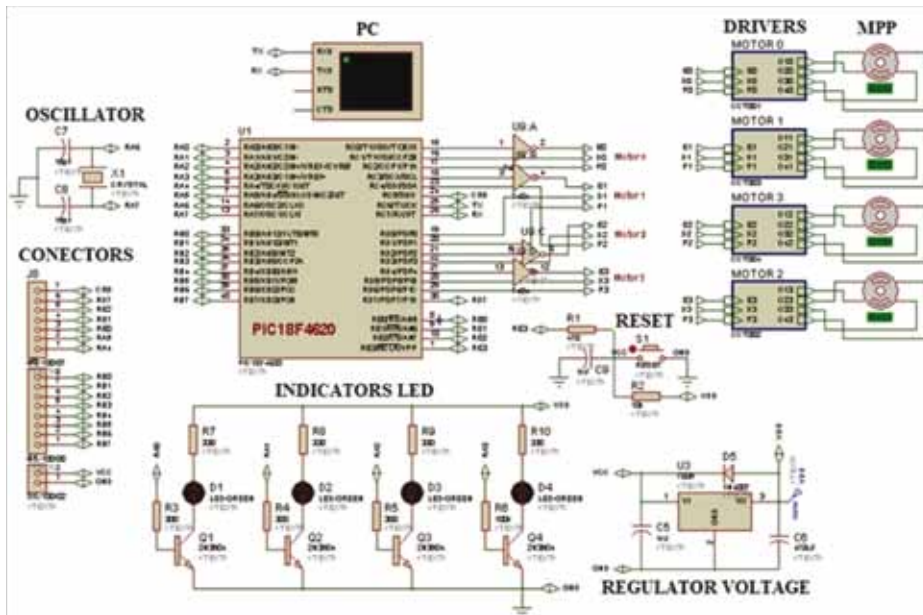
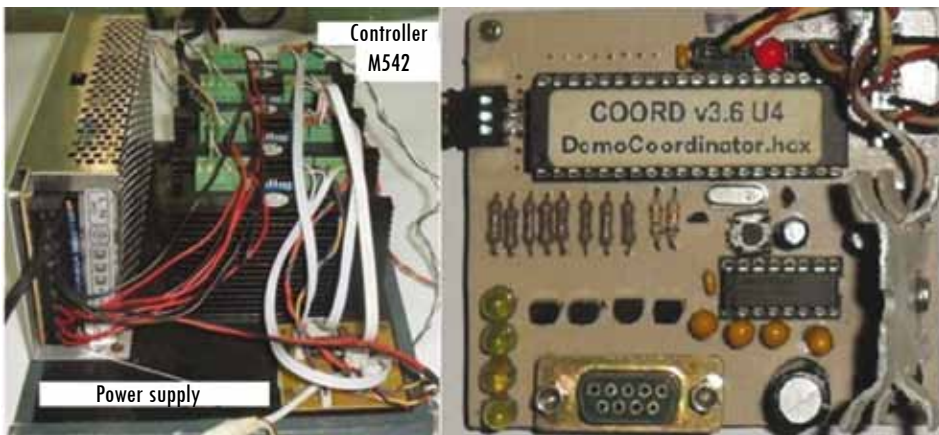


Figure 9. Control exoskeleton module: (A) power supply and controllers, and (B) control board



### 2.2.2. Electromyographic signals acquisition module

Figure 11 shows a block diagram of the process of acquisition for electromyographic signals (EMG). The myoelectric signal acquisition was performed using surface Ag-AgCl electrodes positioned on the agonist and antagonist muscles.

The signals acquired by the sensors are conditioned with an instrumentation amplifier AD620, which has high rejection of common mode interference ( $\geq 100$  dB for the band of interest and a gain equal to 10) (Delisle et al., 2007; (Blanco et al., 2008). Its characteristics allow interference from other sources to be reduced. Subsequently, the myoelectric signal is filtered using a band-pass (20 Hz – 500 Hz) filter, amplified and conditioned to the dynamic range of the analog-digital converter, embedded in microcontroller. The resolution of the converter is 12 bits and the sampling frequency used of 1 kHz.

Figure 10. Firmware flow diagram for configuration and control implementation in the MPP

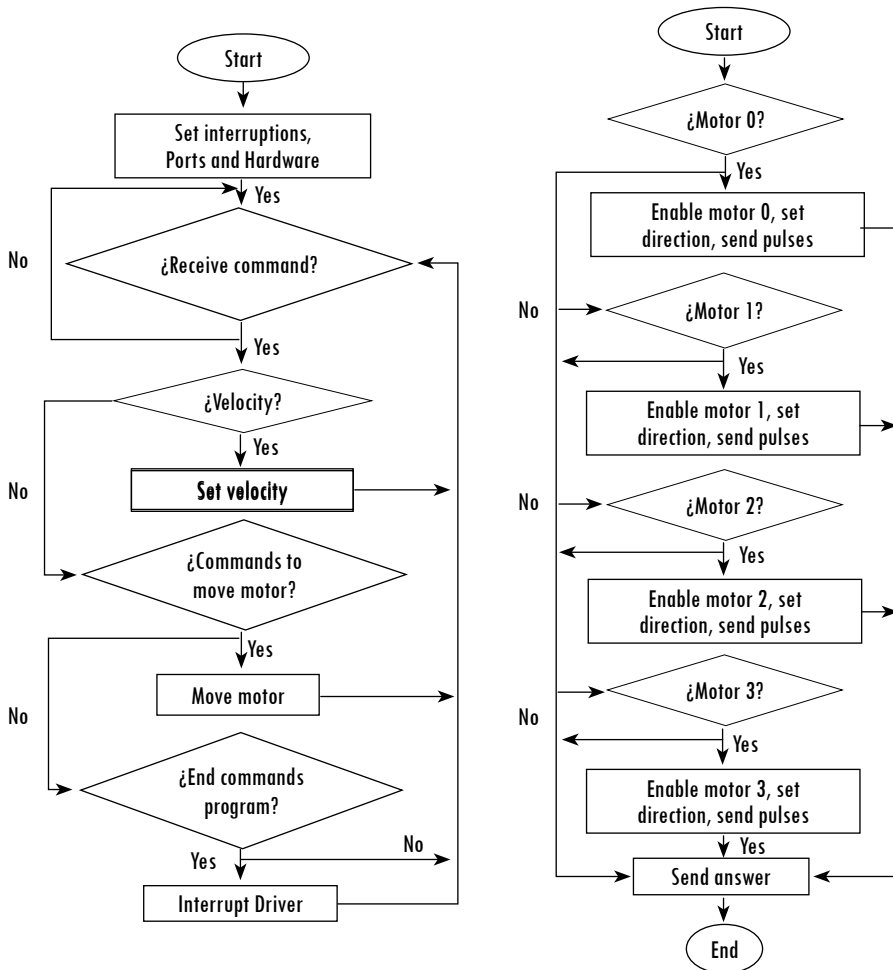
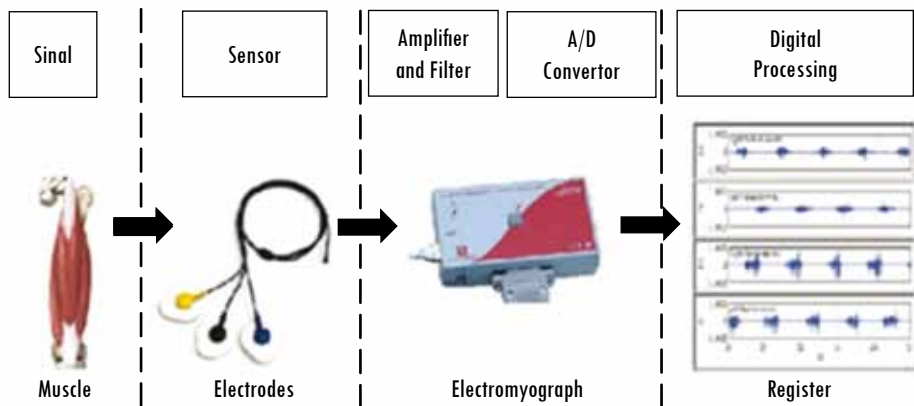


Figure 11. Block diagram of the acquisition process



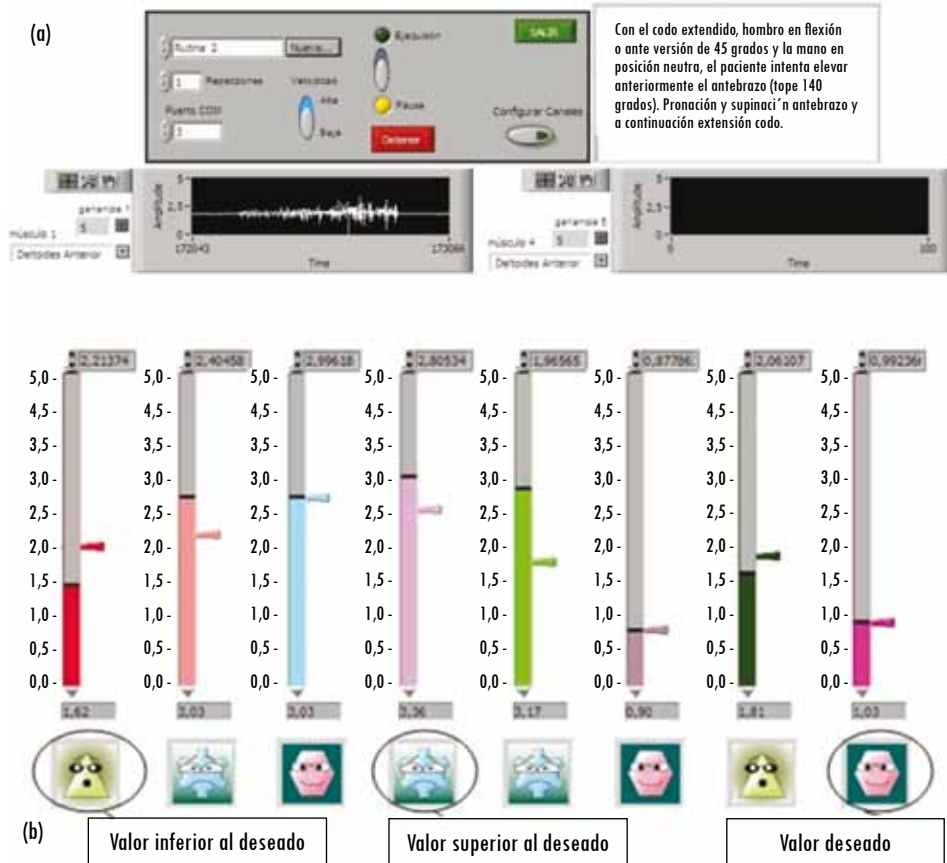
### 2.2.3. Description of the proposed interface

The control interface with electromyography biofeedback techniques for the exoskeleton was implemented in LabVIEW v8.6 software professional. It is provided with a main panel divided into the following sections: selector, editor of motion routines and graphic display of the myoelectric activity. As shown in Figure 12a aspects such as the selection of the desired routine, speed selector and number of repetitions are considered, in addition to enable the option to include new routines according to the degrees of freedom implemented. In biofeedback process three options of graphical interfaces allow the interaction with the patient. One of these variants has animated interfaces during the rehabilitation process (Figure 12b).

The designed interface also allows the configuration of the EMG channels used during the acquisition process, the gain configuration and selection of the corresponding muscles on each channel. While selecting muscles, the therapist can be accompanied by a human map provided with different views and locations associated with surface electrodes in bipolar configuration (Figure 13). All configurations can be stored by the system.

The second (Figure 14) and third (Figure 15) permit to visualize the variation of raw EMG signal and its envelope, respectively. These alternative graphs allow the physiotherapist and the patient to know the start and end of muscle activation and the amplitude values the signal.

Figure 12. (a) Biofeedback techniques main panel interface, and (b) Myoelectrical signal amplitude according to the position the bar code



Processing EMG signals is based in the preprocessing the acquired signal, the envelope detection and calculation of the muscle activation amplitude. The method used for this purpose in this work is the root mean square, see Figure 15. This parameter characterizes the signal according to the estimate energy, related to the amplitude at a certain time interval and represents the average power of signal.

Figure 13. Configuration Window EMG channels

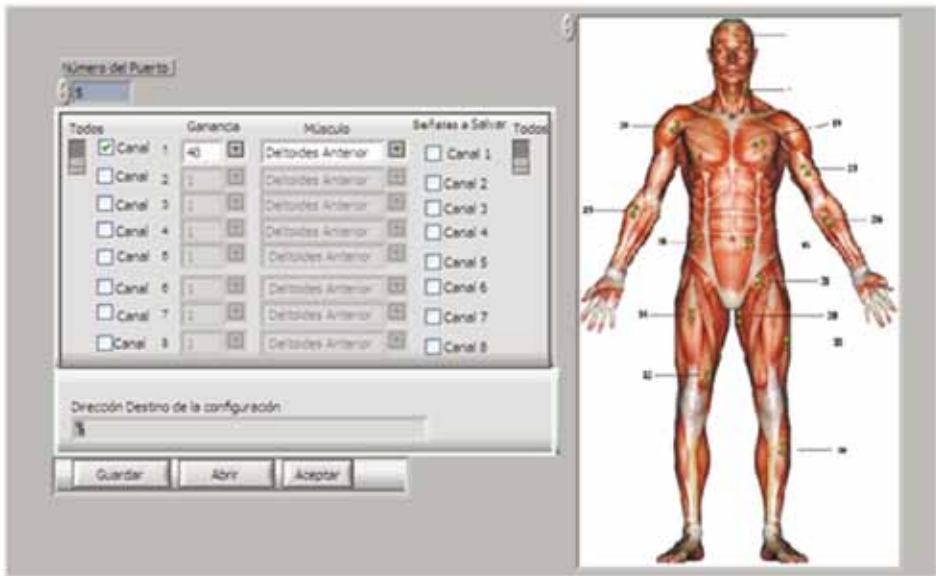
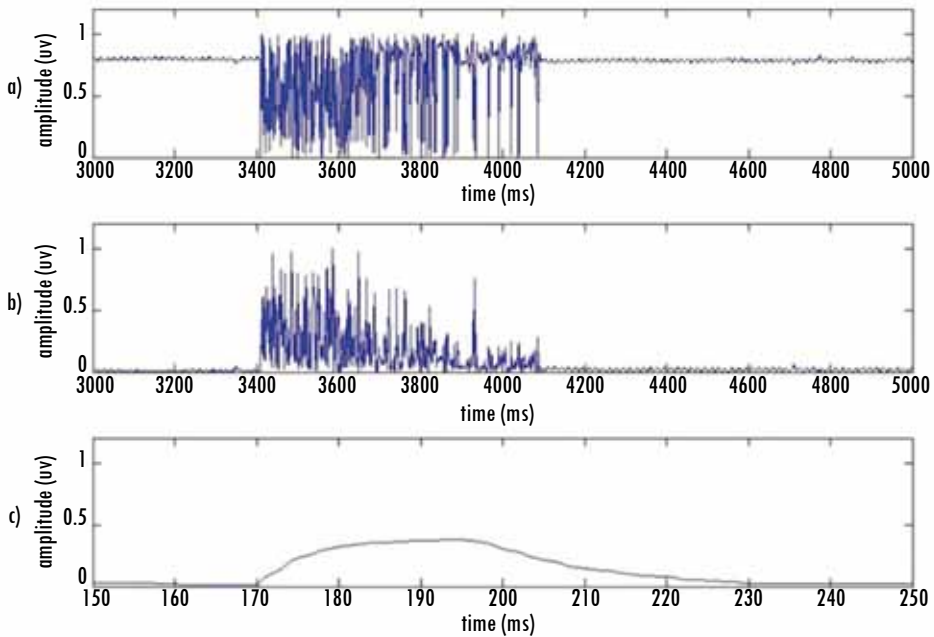


Figure 14. Myoelectric signal captured in the anterior deltoid muscle



Figure 15. Calculate the root mean square: (A) filtered signal, (B) rectified signal envelope, and (C) signal



## Conclusions

According to one therapeutic routine, considering clinical environment, using 4 degrees of freedom and using the possibility of combining these movements for rehabilitation of the upper limbs; the developed mechanical system is able to simulate the kinematics required regarding movements and is adjustable in functional parameters. The presented interface allows control of the movements of the exoskeleton, and the configuration of the analog channels EMG prototype. The implemented functions allow communication with the exoskeleton's control board and EMG prototype. Digital processing methods were tested and showed their effectiveness for detecting the envelope of the EMG signal that is used for patient biofeedback. The next steps are directed towards the implementation of a clinical protocol in subjects presenting muscle dysfunction in the upper limb, with the objective of evaluating the results derived from manual therapy and made from the passive control.



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## References

- AGUIRRE-OLLINGER, G. and COLGATE, J. E. Design of an active one-degree-of-freedom lower-limb exoskeleton with inertia compensation. *The International Journal of Robotics Research*. 2010. DOI: 10.1177/0278364910385730.
- BLANCO, R.; DELISLE, D.; GARCÍA, J.C.; DÍAZ, C., and LÓPEZ, N. Registrador de electromiogramas destinado a estudios de la marcha. *Bioingeniería y Física Médica Cubana*. 2008, vol. 9, no. 3.
- BRAUNE, W. *Determination of body moments of inertia of the human body and its limbs*. Berlin: Springer-Verlag, 1988.
- CENCIARINI, M.; DOLLAR, A. Biomechanical considerations in the design of lower limb exoskeletons. *IEEE International Conference on Rehabilitation Robotics Rehab Week Zurich*, 2011. ETH Zurich Science City, Switzerland, June 29 - July 1, 2011.
- DELISLE, D.; BLANCO, R.; GARCÍA, J.C.; DÍAZ, C.; LÓPEZ, N.; MARTÍNEZ, A. Módulo digital para electromiógrafo portátil. *Ciencia y Tecnología*. 2007, vol. 11, pp. 173-178.
- ESTÉVEZ, A. Grado de discapacidad en pacientes hemipléjicos del "Policlínico Docente Universitario del Cerro". *Revista Cubana de Medicina General Integral*. 2012, vol. 28, no. 4, pp. 682-693.
- HUI, Y. Controlling a powered exoskeleton system via electromyographic signals. *Proceedings of the 2009 IEEE International Conference on Robotics and Biomimetics December 19 -23, 2009, Guilin, China*. pp. 349-353.
- LO, H.S. and XIE, S.Q. Exoskeleton robots for upper-limb rehabilitation: State of the art and future prospects. *Med Eng Phys*. 2011. DOI: 10.1016/j.medengphy.2011.10.004.
- ROSEN, J. and MOSHE, B. A myosignal-based powered exoskeleton system. *IEEE Transaction on Systems, Man, and Cybernetics—part A: SYSTEMS AND HUMANS*. 2001, vol. 31, no. 3.
- SAFIZADEH, M. R. and HUSSEIN, M. Kinematic analysis of powered lower limb orthoses for gait rehabilitation of hemiplegic and hemiparetic patients. *International Journal of Mathematical Models and Methods in Applied Sciences*. 2011, vol. 5, no. 3, pp. 490-498.
- STAUBLI, P. Effects of intensive arm training with the rehabilitation robot ARMin II in chronic stroke patients: four single-cases. *Journal of Neuro Engineering and Rehabilitation*. 2009, vol. 6, no. 46. DOI: 10.1186/1743-0003-6-46.
- USER'S MANUAL for M542 V2.0. *High performance microstepping driver*. Version 1.0, 2008.

WEGE, A. and ZIMMERMANN, A. Electromyography sensor based control for a hand exoskeleton. *Proceedings of the 2007 IEEE International Conference on Robotics and Biomimetics December 15 -18, 2007, Sanya, China.*

WINTER, D.A. *Biomechanics of human movement*. New York: John Wiley and Sons, 1979.